Dec. 1, 1959 Y. LE MASSON

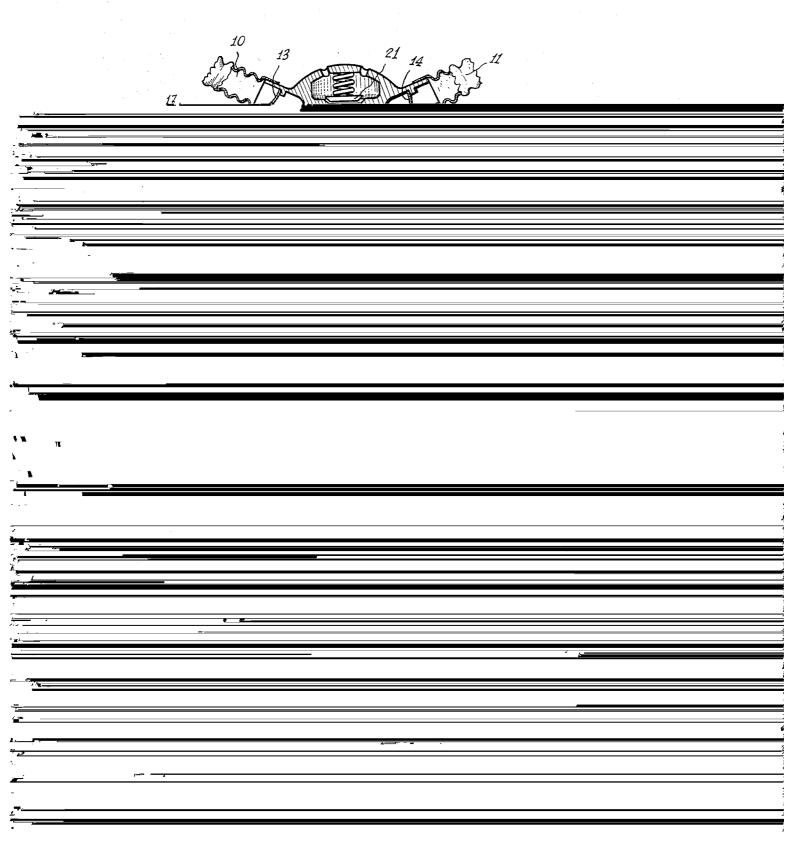
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AUTONOMOUS CLOSED-CYCLE DIVING APPARATUS

Filed July 18, 1956

2 Sheets-Sheet 1

## FIG.1

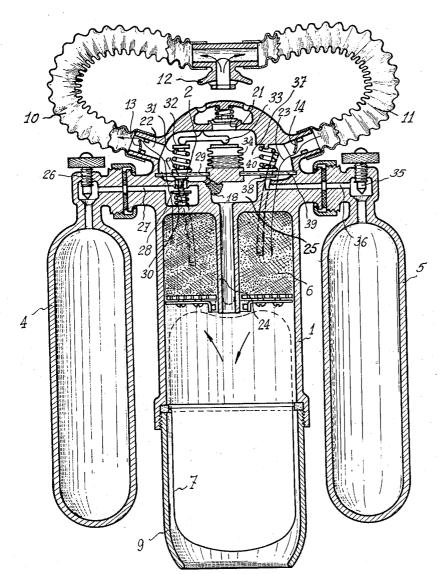


AUTONOMOUS CLOSED-CYCLE DIVING APPARATUS

Filed July 18, 1956

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FIG.2



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## AUTONOMOUS CLOSED-CYCLE DIVING APPARATUS

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Application July 18, 1956, Serial No. 598,664 Claims priority, application France July 19, 1955 10 Claims. (Cl. 128—142)

This invention relates to diving apparatus. The objects of the invention include providing an improved diving apparatus or suit of the autonomous type operating on a closed-cycle principle. More particularly, the device should be lightweight, usable at comparatively great diving depths and for long diving periods, and should provide the diver with the possibility of normal breathing regardless of the depth at which he is positioned and without requiring him to effect manual adjustments during the dive.

A feature of the invention is that the artificial breathing mixture or atmosphere in the closed cycle is contained in a "false lungs" device, i.e. a variable storage tank de-

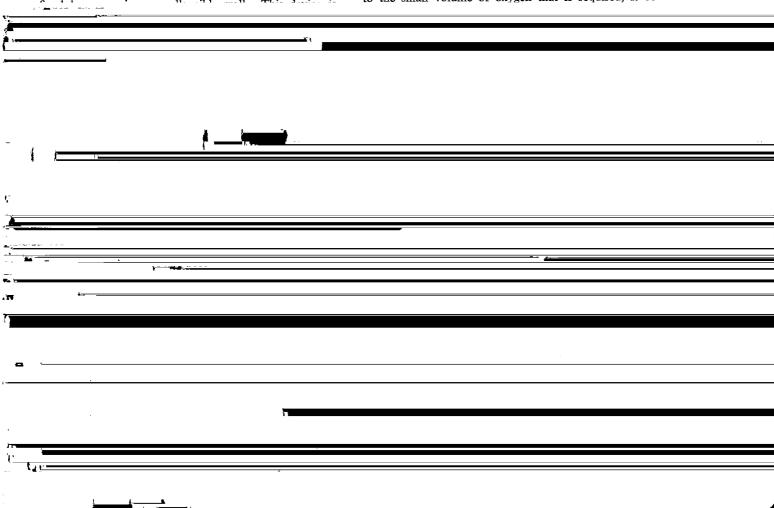
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For a given mass of blood in the body, there corresponds a predetermined oxygen concentration necessary for maintaining life. It follows from the foregoing that this oxygen consumption rate is of the order of 1 cg. per second and corresponds to what will hereinafter be termed "concentration 1." This is a constant independent of ambient pressure.

The problem therefore is to control, with an increasing pressure of the medium, the mass of oxygen consumed per second in such a way that it will be at least equal to the required quantity (concentration 1) while remaining less than the lethal limit (concentration 9 or 10).

The principle on which the autonomous closed-cycle diving apparatus of the invention is based, resides in the recognition of the above disclosed physiological phenomena and laws, and in the provision of an automatic oxygen-regulating mechanism operative to satisfy, at all times, the requirements set thereby.

In addition to the above considerations, it should be noted that, underwater, the average respiratory rhythm is about one inhalation every two seconds, which corresponds to an oxygen consumption per inhalation, taking concentration 1 as a basis, equal to 2 centigrams, or a volume of 0.014 liter at atmospheric pressure. Since the average lung capacity is 2 liters, it is seen that owing to the small volume of oxygen that is required, it be-



per second, the actual quantity that is required in practice at any given time varies with the muscular exertion, respiratory capacity, and like factors, so that a lack or an excess of oxygen might result. A lack of oxygen is not permissible. An excess of oxygen on the other 5 hand will result in a regular increase in the respirable volume which, as stated above, it is desired to retain constant. Consequently, there is no satisfactory operation of the system out of water, since the unconsumed oxygen in excess will then escape through the overflow 10 central body 1, having secured to or integrally formed valve. In this sense, the system will not then operate in a closed cycle.

Now assuming that the apparatus thus adjusted is lowered to a depth of say 10 meters, the pressure increases to two atmospheres and the above-mentioned volume 15 (two liters at 1 atmosphere) is reduced by half and makeup gas is automatically added to it by the means (3) to maintain the volume the same. The respirable volume therefore still remains the same, i.e. equal to the capacity of the user's lungs. But since on the other hand the 20 oxygen absorption capacity of the user has been increased tenfold (concentration 10) the excess of oxygen which occurred at surface conditions, is now taken up. The system operates in a fully closed cycle, so long as the oxygen concentration does not exceed the user's absorption capacity.

The upper limit of concentration at moderate depths is determined by the depth. Beyond 9 meters depth the concentration may be chosen freely, provided it be selected within the range of from 1 to 10.

With the apparatus operating at constant depth, only the means (1) and (2) are operative. When the apparatus is lowered to greater depths, the means (1), (2) and (3) operate. When the apparatus is raised, the volume increases and the means (1), (2) and (4) become 35

The means (1) for insuring constant rate of oxygen delivery may comprise a simple expansion valve followed

tional amount of the gas without any effort on the part of the diver's lung muscles.

Two alternative embodiments of diving apparatus according to this invention will now be described for purpose of illustration but not of limitation with reference to the accompanying diagrammatic drawings wherein:

Fig. 1 is a sectional view of one embodiment of the invention; and Fig. 2 is a similar view of a modification.

As shown in Fig. 1, the diving apparatus comprises a with it a pair of expansion units or valves 2 and 3 supplied with pure oxygen and neutral gas respectively from the storage containers 4 and 5. Each expansion valve may be of a conventional kind including a diaphragm acting on a valve, one side of the diaphragm being actuated by the gas pressure on the downstream or delivery side while the other side of the diaphragm receives the combined action of the pressure of the ambient medium and of an adjustable biassing spring.

The body 1, into which the expanded oxygen and neutral gas are delivered from the units 2 and 3, is connected with a reservoir 6 containing a substance adapted to absorb carbon dioxide gas, such as soda lime or another suitable absorber of CO2. The body 1 is further connected with the interior space of a "false lung" device or collapsible container 7. This may comprise a bag or tank defined by a fluid-tight, flexible wall having a circular orifice 8 sealed between the body 1 and a protective hood 9 of generally cylindrical shape having one end screwed into the body 1. The outer end of the hood may be hemispherical and is perforate so as to allow the surrounding medium, water, to contact the outer face of the bag 7 of the false lung during a dive.

The false lung 7 is adapted to move from the expanded full-line position to the retracted or collapsed position shown in chain lines, and in so doing the capacity of the lung changes by about 3 liters.

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ciently collapsed to actuate the trigger 20. Thus, the valve 3 remains inoperative to supply make-up gas. If the depth and pressure increase, the volume of respirable mixture decreases, and as the diver fills his lungs with the mixture, the false lung 7 collapses sufficiently to open the valve 19 and feed in an additional amount of neutral gas which will again maintain the volume of gas at a value corresponding to the capacity of the diver's lungs. If, on the other hand, the depth and external pressure decrease, the internal gas increases in volume but, since 10 the maximum volume offered to it as determined by the fully expanded condition of the bag 7 is limited there is an excess of internal pressure over the pressure of the external medium, and the excess of mixture escapes through the valve 21.

All of the above operation is of course fully automatic throughout the diving process which may be continued until exhaustion of the oxygen store or that of the absorbing capacity of the reservoir.

The embodiment shown in Fig. 2 also comprises a 20 body 1 the interior of which communicates with the false lung 7 and also with the reservoir 6 containing carbon dioxide absorptive material.

Just as in the first embodiment, the reservoir 6 is connected by the conduits 22 and 23 via chamber C with the 25 flexible tubes 10 and 11 serving respectively for the outlet and inlet of the breathing mixture, and each of which is fitted with a check valve 13 or 14. Extending through the reservoir 6 is a conduit 24 connected at its ends with the interior of body 1 and with a chamber 25 respectively.

The oxygen tank 4 is connected to the chamber 25 by way of a manually-operable needle-valve 26, a conduit 27, a valve generally designated 2, and a jet orifice 18. The valve 2 comprises gas-pressure operated system including a valve 28 controlled by a diaphragm 29. One side of the diaphragm 29 is subjected to the combined action of the downstream gas pressure and a bias spring 30 which tend to urge the valve to its sealing position, while the other side of the diaphragm receives the action of the external pressure and an adjustable spring 40 31 urging the valve to open position. The spring 31 engages a stop 32 engaged by one end of a lever 33. The other end of the lever is actuated by a barometric capsule or bellows 34 partially filled with liquid under pressure.

The chamber 25 may moreover be placed in communication with the tank 5 of neutral gas by way of a handoperated needle-valve 35, a conduit 36 and a check-valve which may be considered as an expansion valve mounted in inverted relation, and generally designated 37. The 50 actuating means comprises a mechanical linkage. valve includes a check-valve member 38 connected with a diaphragm 39. One side of this diaphragm is acted upon by the pressure in chamber 25 acting to open the valve, while the other side of the diaphragm receives the combined action of the external pressure and a biassing 55 spring 40 acting to close the valve.

When the diver is positioned at a given depth, oxygen flows at a constant rate into chamber 25 and, through conduit 24, into the body 1. Should the diving depth increase, the oxygen flow rate would tend to increase. However, the increase in external pressure due to the increase in depth will cause a collapse of the capsule 34 and hence a reduction in the compression stress of biassing spring 31. This reduction in the compression of the spring offsets the effect of the increase in external pressure on the expansion valve, so that the delivery rate of oxygen can be maintained at a strictly constant value regardless of the external pressure by suitably dimensioning the barometric capsule 34.

The valve 38 is normally maintained seated by spring 70 40 so that the delivery of neutral gas is cut off. As the outer pressure increases, the volume of gas within the false lung increases and, at a predetermined point in the operation, the wall of the lung engages the end of the conduit 24 towards the end of an inhaling action, so that 75

the conduit is sealed off. Since oxygen continues to flow into chamber 25, the pressure in the chamber rises, unseating valve 38 and thus resulting in a supply of makeup neutral gas into the respiratory circuit. It will be observed that, in contrast to what occurs in the embodiment of Fig. 1 the diver does not have to expend any additional muscular effort to open the valve, since the valve opening is produced pneumatically by the pressure obtaining in chamber 25.

What I claim is:

1. In a diving device, a collapsible container having a flexible wall, means for connecting in a closed circuit said container with the respiratory organs of the user of said apparatus, means for delivering oxygen into said con-15 tainer at a substantially constant rate, and means for maintaining the volume of respirable mixture in said closed circuit substantially constant.

2. In a diving device, a collapsible container having a flexible wall, means for connecting said container with the respiratory organs of a diver in a closed circuit, means for delivering oxygen into said container at a substantially constant rate, means responsive to surrounding pressure and to said collapsible container for supplying neutral-gas into said container when said pressure increases and means coupled to said container for discharging excess respirable mixture from said container when said pressure decreases.

3. In a diving device, a collapsible container having a flexible wall, inhaling and exhaling conduits for connecting said container with the respiratory organs of a diver in a closed circuit, a tank of oxygen gas coupled to said container, a tank of neutral-gas, means connecting said neutral-gas tank with said container including a valve biassed to closing condition, actuating means connected with the valve and responsive to said collapsible container to open the valve and deliver neutral gas into said container, and relief valve means connecting said container with the exterior, whereby said closed circuit will contain at all times a substantially constant volume of respirable mixture.

4. The combination claimed in claim 3 comprising an expansion valve connected with said oxygen tank and a jet orifice connected with the expansion valve to deliver expanded oxygen at a substantially constant rate into 45 said container.

5. The combination claimed in claim 4 comprising manual adjusting means for variably biassing said expan-6. The combination claimed in claim 5, wherein said

7. The combination claimed in claim 5, wherein said actuating means comprises a gas-pressure operated system.

8. The combination claimed in claim 5, wherein said actuating means comprises a chamber coupled to the first said means, a fluid passage between said chamber and said container and positioned to be engaged by said flexible wall to be sealed thereby, and means responsive to the pressure in said chamber for operating said expansion valve.

9. The combination claimed in claim 4 comprising adjustable spring bias means for the expansion valve, and an element responsive to external pressure and operative to adjust said bias means in accordance with said external pressure.

10. The combination claimed in claim 4, wherein said neutral-gas is selected from the group consisting of hydrogen and helium.

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